

Editorial

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# Enzyme replacement therapy: current challenges and drug delivery prospects via extracellular vesicles

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Lysosomal storage disorders (LSDs) comprise > 70 inborn errors of metabolism that are individually considered rare diseases but all together concern 1 in 5000 live births<sup>[1]</sup>. LSDs are caused by defects in genes related to the lysosomal homeostasis. This results in the abnormal storage of macromolecules in cells, triggering chronic inflammation<sup>[2]</sup>. About 70% of LSDs feature neurodegenerative damage<sup>[3]</sup>. Therapeutic strategies comprise gene therapy, therapies based on small molecules (i.e., chaperones), organ/cell transplantation (bone marrow transplantation), substrate reduction therapy, and enzyme replacement therapy (ERT)<sup>[4]</sup>. At present, the most important clinically approved therapy for several LSDs is ERT<sup>[5]</sup>.

ERT is based on the periodic life-long intravenous administration of specific enzymes purified from cells engineered for their specific production with recombinant DNA technology, to palliate impaired enzyme function in patients<sup>[5,6]</sup>. Since the first ERT was clinically approved for Gaucher disease ( $\beta$ -



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glucocerebrosidase deficiency) in 1991, several other enzymes have been approved for clinical use [Table 1]. ERT is a costly therapy reaching about \$200,000/year<sup>[4]</sup>.

ERT's current challenges are multiple. They include the following.

**Safety and efficacy:** An important issue concerning ERT relates to the immune response exerted against these biologicals. This issue was highlighted by the FDA, indicating the need for investigations on monitoring tests and therapy optimization<sup>[11]</sup>. The neutralizing antibodies can reduce the therapeutic outcome of ERTs as they can bind to the enzyme active site and/or ligands involved in the interaction with a receptor on the cells of interest, blocking the cellular uptake<sup>[12]</sup>. Therefore, patient immune response to the frequent enzyme administration ultimately affects ERT safety and/or treatment efficacy. This is especially relevant in the case of Pompe disease, as newborns developing antibodies do not respond to treatment and have no other treatment option.

**Tissue targeting:** Reaching the central nervous system (CNS) is one of the main challenges of ERT in order to provide effective therapy for most of the disease conditions. Indeed, recombinant enzymes infused intravenously fail to cross the blood-brain barrier (BBB) and access the CNS<sup>[13]</sup>. Large, polar molecules such as the recombinant enzymes used for ERT are poorly amenable to cross the BBB<sup>[14]</sup> and enzymes engineered to display an increased brain endothelium transcytosis by fusion with a monoclonal antibody directed against a brain endothelium receptor, e.g., insulin or transferrin receptors, are currently under clinical investigation for MPS<sup>[15]</sup>. ERTs are clinically approved for very few diseases [Table 1]. For the clinically approved ERTs, the main targets are peripheral sites. Once in the circulation, the administered enzymes feature a short half-life. The major proportion of the administered recombinant enzymes is distributed to the visceral organs<sup>[5,6]</sup>.

**Cellular targeting:** Enzyme delivery to its cellular and/or subcellular (lysosomal) targets is an additional challenge. In the case the enzymes are insufficiently or not properly glycosylated, there may be an impairment in their ability to bind receptors, enter the cells, and reach their lysosomal target. These post-translational modifications are a limiting factor in the production of enzymes for ERT<sup>[4]</sup>. Additionally, the high expression levels of the mannose receptor in the liver also render difficult ERT delivery to tissues where it is the most needed such as macrophages in Gaucher disease<sup>[16]</sup>.

**Restriction to soluble enzymes:** ERT based on the infusion of a purified enzyme is not relevant for LSDs arising from mutations in lysosomal membrane proteins such as CLN3 because large-scale purification of active membrane proteins is technically challenging and requires a lipidic or lipid-like environment.

ERT may fail to provide the expected therapeutic effect considering not only its non-specific biodistribution but also its low bioavailability due to a high biodegradation rate<sup>[17]</sup>. There is a real need in ERT for the design of targeted delivery systems combining both efficacy and safety to protect and address enzymes.

Enzyme encapsulation in nanosystems can overcome key challenges in ERT, including undesired immunologic reactions and biodegradation. It can also prevent non-selective biodistribution and improve the pharmacological response by increasing the drug absorption, enzyme controlled release, pharmacokinetics, and pharmacodynamics properties<sup>[17]</sup>. Current ERT nanomedicine research has focused on polymeric nanoparticles<sup>[18]</sup>, liposomes<sup>[19]</sup>, and other platforms such as protein aggresomes<sup>[20]</sup>. The liposomal strategy was reported by Cabrera *et al.* for Fabry disease<sup>[21]</sup> and by others for Batten disease<sup>[19,22]</sup>. More recently, extracellular vesicles (EVs) have been proposed as a bio-platform for ERT delivery for

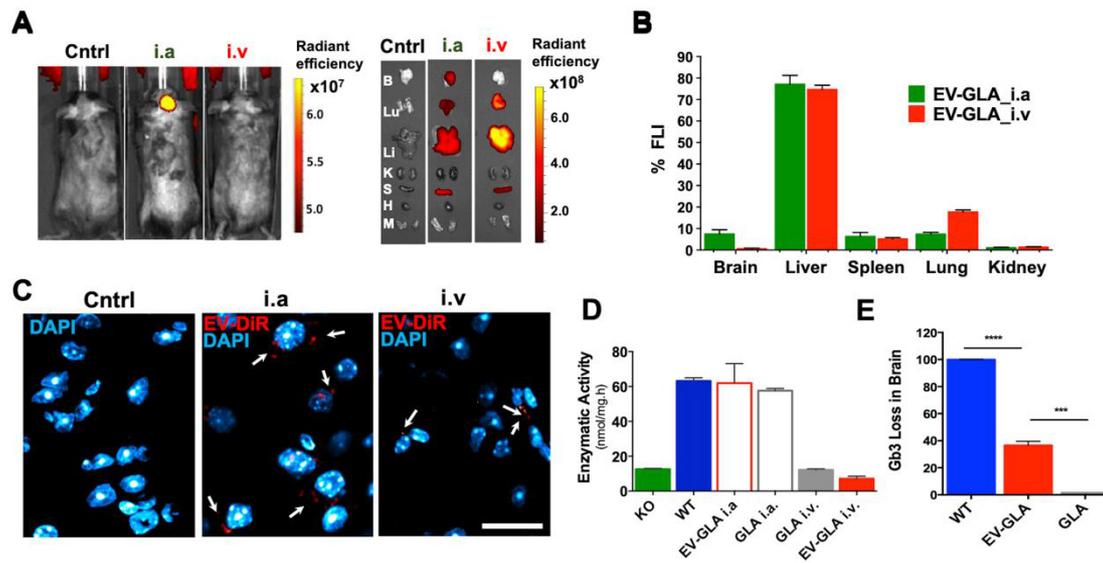
**Table 1. Enzyme replacement therapy clinically available or under evaluation (updated from Refs.<sup>[4,7-10]</sup>)**

Disease (deficient enzyme)	ERT	Approval for clinical use (year/regulatory agency)
Gaucher's disease ( $\beta$ -glucoce-rebrosidase)	Velaglycerase (VPRIV™)	2010-FDA, EMA; 2014-PMDA
	Taliglycerase (Eleyso™)	2012-FDA
	Imiglycerase (Cerezyme®)	FDA-1991, EMA-1997
Fabry disease ( $\alpha$ -galactosidase)	Agalsidase $\alpha$ (Fabrazyme™)	2001-EMA
	Agalsidase $\beta$ (Replagal™)	2003-FDA, EMA
	PRX-102 (pegunigalsidase alfa)	Submitted in 2022 to EMA
Pompe disease ( $\alpha$ -glucosidase)	Aglucosidase (Myozyme™)	2006-FDA, EMA, PMDA
	Aglucosidase (Lumizyme™)	2010-FDA
	Avalglucosidase alfa (Nexviazyme®)	EMA-2021, FDA-2021
MPS I (Hurler syn.) ( $\alpha$ -L-iduronidase)	Laronidase (Aldurazyme™)	2003-FDA, EMA; 2006-PMDA
MPS II (Hunter syn.) Iduronate-2-sulfatase	Idursulfase (Elaprase™)	2006-FDA; 2007-EMA, PMDA
MPS IV A (Morquio A syn.) (N-acetylgalactosamine 6-sulfatase)	Elosulfase Alfa (Vimzim™)	2014-FDA
MPS VI (Maroteaux-Lamy syn.) (arylsulfatase B)	Galsulfase (Naglazyme™)	2005-FDA; 2006-EMA; 2008-PMDA
Lysosomal acid lipase deficiency (Lysosomal acid lipase)	Sebelipase $\alpha$ (Kanuma™)	2015-FDA, EMA; 2016-PMDA
CLN2 deficiency -> Brineura (2017)	cerliponase alpha (Brineura®)	2017-FDA and EMA
mucopolysaccharidosis type VII (MPS VII)	Vestronidase alfa (Mepsevii™)	2017-FDA and EMA-2018
Gaucher disease ( $\beta$ -glucocerebrosidase deficiency)	Imiglycerase (Cerezyme®)	FDA-1991, EMA-1997

FDA: Food and Drug Administration; EMA: European Medicines Agency; PMDA: Pharmaceuticals and Medical Devices Agency.

Gaucher disease<sup>[23,24]</sup>. EVs, encompassing exosomes, microvesicles, and apoptotic bodies, are sub-cellular entities (40-5000 nm diameter) secreted by cells in a constitutive or inducible manner<sup>[25-27]</sup>. Importantly, more than conferring enzyme protection, EVs may enable enzymes to reach the CNS as EVs are able to cross the BBB<sup>[28,29]</sup>.

Seras-Franzoso *et al.* reported the feasibility of EVs for both Fabry and Sanfilippo diseases. They demonstrated that EVs released by CHO DG44 and HEK293 cells transfected with plasmids coding for alpha-galactosidase A (GLA) or N-sulfoglucosamine sulfohydrolase (SGSH) enzymes (defective in Fabry and Sanfilippo A diseases, respectively) were constitutively loaded with these enzymes<sup>[30]</sup>. This outstanding result means that the expression system spontaneously released the enzyme directly in the biogenic vesicle delivery platform. Of note, both lysosomes and some EVs stem from the multivesicular endosomes (MVE), which may explain the high concentration of GLA and SGSH enzyme within the EVs. *In vitro* data demonstrate that GLA-loaded EVs were rapidly internalized and reached the lysosome sub-cellular target in cellular models of Fabry disease, inducing a therapeutic effect superior to the clinically used recombinant enzyme. The biodistribution of EV-GLA labeled with florescent DiR dye was investigated in a Fabry KO mice. EV-GLA were able to cross the BBB when administered intraarterially (i.a.) by canulation of the external carotid or intravenously (i.v.) by tail vein injection [Figure 1A and B]. *Ex vivo* images obtained by confocal microscopy indicated that the fluorescent signal of EV-GLA reached brain parenchyma after i.a. administration and, to a smaller extent, after i.v. administration [Figure 1C]. The enzymatic activity of GLA was measured in brain tissues 1 h post i.v. administration. Treated animals exhibited basal enzymatic activities, comparable to the K.O. animals [Figure 1D]. However, there are some sensitivity limitations regarding the techniques for measuring GLA activity and brain biodistribution. Therefore, the authors also evaluated the levels of globotriaosylceramide (Gb3, the enzyme substrate) in mice one week after a single i.v. administration of GLA and EV-GLA (1 mg/kg of GLA, Figure 1E). Remarkably, the results indicate that EV-GLA induced a significant reduction in Gb3 deposits in contrast to free GLA. Overall, these results



**Figure 1.** EV-GLA therapeutic effect. (A) *In vivo* (left) and *ex vivo* (right) fluorescence imaging (FLI) of Fabry KO mice treated with either intraarterial (i.a.) or intravenous (i.v.) administration of DiR-labeled EV-GLA (1 mg/kg of GLA) in comparison to the non-treated controls (Cntrl). (B) FLI signal quantification to compare the biodistribution of EV-GLA following i.v. or i.a. administration. (C) Confocal images of brain parenchyma showing DiR fluorescent signal of EV-GLA (red) and DAPI-labeled cell nuclei (blue). Scale bar represents 20  $\mu\text{m}$ . (D) GLA enzymatic activity 1 h post-administration in brains of Fabry KO mice treated with GLA or EV-GLA via i.v. or i.a. administrations (E) Loss of Gb3 in KO mice that received an i.v. single dose of EV-GLA, as measured by LC-HRMS seven days after dosing (figure used with permission from Figure 5 of Seras-Franzoso *et al.* Available from: <https://doi.org/10.1002/jev2.12058><sup>[25]</sup>). FLI: Luorescence imaging; GLA: alpha-galactosidase A.

indicate that i.v. administered EV-GLA reached the brain parenchyma and induced a therapeutic effect at lysosomes in Fabry KO mice.

Another proof-of-concept of EV efficacy in ERT therapy of LSDs was provided by Haney *et al.* in a preclinical model of Batten disease (BD)/neuronal ceroid lipofuscinosis (NCL)<sup>[31,32]</sup>. NCLs are a group of 14 inherited neurodegenerative disorders of childhood characterized by visual failure, epilepsy, progressive motor and cognitive decline, and premature death. NCLs are multisystemic disorders, but the brain is strongly affected with neurons progressively accumulating in lysosomes an NCL-specific lipopigment (lipofuscin) and some proteins such as the c-subunit of the mitochondrial ATP synthase (SCMA) before dying. In addition, an inflammatory response characterized by reactive astrocytosis is observed in the brain regions affected by the disease. There is currently no curative treatment available for most NCLs, except for type 2 (CLN2), which results from the defective activity of the soluble lysosomal hydrolase TPP1 (tripeptidyl peptidase-1). The approved ERT for CLN2, Brineura<sup>[33]</sup>, significantly reduces motor and language decline in patients<sup>[34]</sup>. However, since the purified enzyme is delivered every two weeks via an intracerebroventricular device, some concerns exist about the long-term efficacy and tolerance of the treatment and alternative solutions are needed. The group of Elena Batrakova showed that macrophage-derived EVs loaded with purified TPP1 efficiently delivered the enzyme to lysosomes in both *in vitro* and *in vivo* models of CLN2. A robust accumulation of EV carriers was observed in the brain of a CLN2 mouse model after intraperitoneal injection<sup>[31]</sup>. Accumulation of storage material, astrocytosis, and neuronal death were reduced, and mouse lifespan was extended<sup>[31]</sup>. A further increase in CLN2 mouse model lifespan was obtained when EV-TPP1 was delivered by a combination of two delivery routes, intraperitoneal and intrathecal injections<sup>[32]</sup>, which target both the brain and peripheral organs. Interestingly, intranasal administration of EV-TPP1 resulted in significant astrocytosis reduction and neuron survival increase<sup>[32]</sup>. This result gives some hope that EV-based therapy could cure brain consequences of CLN2 loss when delivered via a minimally invasive

administration route, an essential point for a lifelong treatment that would start during early childhood.

These encouraging results open a new venue in the field of ERT. Huge prospects may be expected considering that EVs are a versatile drug delivery platform endowed with intrinsic therapeutic properties and enhanced capabilities to cross biological barriers. From a market strategy standpoint, ERT may represent an attractive business niche for EV biotech companies considering treatment costs of ~€200,000 per patient-year. Additionally, the choice of an orphan indication is an asset to obtaining fast feedback from regulatory bodies. This would, to some extent, facilitate the entry of EV-based medicines in clinical trials with fewer patients, high reimbursement, and extended protection.

## DECLARATIONS

### Authors' contributions

Wrote the paper: Silva AKA, Sagné C

Revised the paper providing remarks for its improvement: Gazeau F, Abasolo I

### Availability of data and materials

Not applicable.

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### Conflicts of interest

Gazeau F and Silva AKA are co-founders of the spin-off Evora Biosciences. Silva AKA is co-founder of the spin-off EverZom. The other authors have no conflicts to declare.

### Ethical approval and consent to participate

Not applicable.

### Consent for publication

Not applicable.

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